

1 **ABSTRACT**

2 With great interest, our independent groups of scientists located in Korea and Germany
3 recognized the use of a very similar methodological approach to quantify the uptake of
4 radioactive glucose (^{18}F -FDG) at the cellular level. The focus of our investigations was to
5 disentangle microglial ^{18}F -FDG uptake. To do so, CD11b immunomagnetic cell sorting
6 (MACS) was applied to isolate microglia cells after *in vivo* ^{18}F -FDG injection, to allow simple
7 quantification via gamma counter. Importantly, this technique reveals a snapshot of cellular
8 glucose uptake in living mice at the time of injection since ^{18}F -FDG is trapped by hexokinase
9 phosphorylation without further opportunity to be metabolized. Both studies indicated high ^{18}F -
10 FDG uptake of single CD11b positive microglia cells and a significant increase of microglial
11 ^{18}F -FDG uptake when this cell type is activated in the presence of amyloid pathology.
12 Furthermore, another study investigated noticed that MACS after tracer injection facilitated
13 determination of high ^{18}F -FDG uptake in myeloid cells in a range of tumor models. Here, we
14 aim to discuss the rationale of single cell radiotracer allocation via MACS (scRadiotracing) by
15 providing examples of promising applications of this innovative technology in neuroscience,
16 oncology and radiochemistry.

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18 **MAIN TEXT**

19 **Potential applications of scRadiotracing in neuroscience**

20 Spatiotemporal alterations of the ^{18}F -FDG-PET signal comprise a well-established
21 read-out in the diagnostic workup of patients with neurological disorders (1-3). However, the
22 method lacks the cellular resolution to distinguish respective contributions of different cell types
23 to the ^{18}F -FDG uptake. The majority of earlier studies claimed that neuronal activity and
24 neuronal ^{18}F -FDG uptake dominate glucose uptake and consumption in the mammalian brain
25 (4). However, several recent studies highlighted a significant contribution role of glial cells for
26 the energy metabolism of the brain (5-7), which questions ^{18}F -FDG-PET as a pure biomarker
27 of neuronal activation (8). We applied immunomagnetic cell sorting after *in vivo* radiotracer
28 injection and brain extraction, followed by subsequent measurement of gamma emission and

1 cell count in enriched cell fractions to calculate radiotracer uptake per specific single cell
2 (scRadiotracing). Subsequently, our two recent studies exploring scRadiotracing technology
3 identified high microglial ¹⁸F-FDG uptake in mouse models with amyloid pathology (7,9) (see
4 Fig. 1 for the workflow). Furthermore, microglial ¹⁸F-FDG uptake comprised the most likely
5 reason of elevated ¹⁸F-FDG-PET signals in these mice (7,9). However, many remaining
6 questions of altered ¹⁸F-FDG-PET signals may also be addressed by an analysis of glucose
7 uptake at cellular resolution. Recently, we discovered a reduction of the ¹⁸F-FDG-PET signal
8 in a progranulin knock-out mouse model with hyperactivated microglia and in a mouse model
9 with homeostatic microglia (Trem2-knock-out) (10). While this finding speaks for reduced brain
10 function in both genotypes, it still remains unclear if progranulin knock-out microglia have lower
11 ¹⁸F-FDG uptake or if the net signal is driven by reduced neuronal activity despite higher ¹⁸F-
12 FDG uptake of activated microglia (7,9). This example illustrates the need to study glucose
13 uptake at cellular resolution. Given the growing evidence for astrocyte-neuron lactate shuttle
14 (11,12), it will be of interest to reveal whether increasing neuronal activity (13) can stimulate
15 glial ¹⁸F-FDG uptake, which could be addressed using scRadiotracing. The presence of such
16 shuttle systems questions the cellular glucose uptake regardless of the individual glucose
17 consumption of different cell types, which is undeniably high in active neurons (14). In this
18 regard, there could be an imbalance between the cellular localizations of glucose uptake and
19 energy consumption. Importantly, scRadiotracing after ¹⁸F-FDG injection could be specifically
20 used to allocate glucose uptake, while other tracers could be used to track metabolites of
21 aerobic and anaerobic glycolysis at the cellular level. Furthermore, uptake mechanisms during
22 acute stimulation of glucose consumption by physiological (15) or pharmacological
23 interventions could be deciphered by scRadiotracing. To this end, task related stimuli could be
24 applied together with resurgent functional PET methodology (16) and scRadiotracing in
25 experimental models. scRadiotracing could be applied after brain extraction at the time-point
26 of maximal stimulation, determined by the functional PET read-out, to track the changes of
27 cellular ¹⁸F-FDG uptake in contrast to unstimulated conditions.

1 As another example in the field of neuroimaging, tau-PET tracers emerged as valuable
2 biomarkers for the differentiation of tauopathies from controls (17). However, the translation of
3 *in vitro* tau-PET tracer binding to an *in vivo* signal is still under debate and the detailed cellular
4 sources of autoradiography and tau-PET signal elevations remained unclear. Hence, our novel
5 scRadiotracing approach could be used to calculate tau-PET tracer uptake at cellular
6 resolution of single neurons and astrocytes in models of tauopathies in order to close this
7 knowledge gap. As a general note, brain subregion analyses by scRadiotracing are also
8 feasible as long as the product of the cellular yield and the tracer abundance exceed the
9 detection limit of the gamma counter. In this regard, we successfully dissected the
10 hippocampus to study region specific 18F-FDG uptake in mice with amyloid pathology (9). In
11 tauopathies, this feature could be used to compare single cell radiotracer uptake of regions
12 with high and low tau abundance.

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14 **Potential applications of scRadiotracing in neurooncology and oncology**

15 The novel combination of tracer injection and immunomagnetic cell sorting could also
16 facilitate dedicated analysis of tumor cells in experimental models of brain tumors together with
17 analysis of specific immune cell fractions and tumor surrounding cells such as neurons and
18 ependymal cells. This could be highly valuable since the target of several tracers for
19 glioblastoma imaging, including the 18kDa translocator protein (TSPO), is not restricted to a
20 single cell type. Determining the radiotracer uptake of TSPO ligands at cellular resolution in
21 brain is of general interest since the target is not specifically expressed by microglia cells but
22 also by tumor cells, astrocytes, endothelial cells and neurons (18). Since blood-brain-barrier
23 disruption is often questioned as a strong influencer of PET tracer signals in brain tumor
24 imaging, scRadiotracing could also act as a proof of cellular radiotracer allocation. Here, the
25 magnitude of radiotracer uptake per cell could be multiplied with respective absolute cell
26 numbers to investigate if the entire PET signal is explained by cellular sources.

1 Apart from brain tumors, the aforementioned oncological investigation (19) already
2 applied scRadiotracing in a wide range of tumor models, including renal cell carcinoma,
3 colorectal carcinoma (CT26, MC38), and breast cancer. Importantly, the authors did not only
4 employ 18F-FDG but also used 18F labelled glutamine to disentangle it's metabolism in tumor
5 cells and the tumor microenvironment (19). This shows that scRadiotracing is not limited to
6 18F-FDG and highlights the broad range of potential scRadiotracing applications in
7 experimental oncology. For example, prostate specific membrane antigen (PSMA) radiotracers
8 are preferred to target prostate cancer cells because they exhibit very low glucose
9 consumption and therefore cannot be detected by 18F-FDG-PET. However, PSMA is not only
10 expressed in prostate cells, but can be found in several other tissues such as nonprostatic
11 epithelial cells, other neoplastic cells, and tumor-associated neovasculature. PSMA uptake
12 was also associated to inflammatory and infectious processes (20). Thus, scRadiotracing
13 could be used to differentiate PSMA uptake in prostatic cancer cells from others and to avoid
14 pitfalls in prostate cancer diagnostics. The same applies to the diagnostics of well differentiated
15 neuroendocrine tumors (NETs) such as gastroenteropancreatic NETs and meningiomas
16 using radiolabeled somatostatin receptor (SSTR) ligands. The importance of NET diagnostics
17 and therapy is underpinned by an interventional multicenter phase III clinical trial (NETTER) to
18 compare peptide receptor radionuclide therapy using $^{177}\text{Lu-DOTA}^0\text{-Tyr}^3\text{-Octreotate}$ to
19 treatment with high dose Octreotide LAR in patients with metastasized or locally advanced,
20 inoperable, SSTR positive, midgut carcinoid tumors. However, SSTR expression is not
21 exclusive for NET or meningioma cells. Tracer uptake was also observed for inflammatory
22 pathologies including cardiovascular disease and ischemia, and various other benign and
23 malignant tumors (21). scRadiotracing has the potential to resolve such inconclusive results
24 by use of back translation in experimental models. This may help to determine off-target
25 sources and prevents false positive findings. In cases with borderline SSTR expression, dual
26 scRadiotracing may also be suitable to elucidate if SSTR radioligands or 18F-FDG are better
27 suited for follow-up PET imaging of the individual patient.

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1 **Potential applications of scRadiotracing in radiochemistry and radiotracer development**

2 scRadiotracing might also be a versatile tool in tracer development to investigate cell
3 specific uptake of acutely isolated cells when compared to cell culture where metabolic activity
4 of cells may be altered. In general, *ex vivo* radiopharmaceutical research methods mostly rely
5 on macroscopic samples for quantification in a gamma counter or on autoradiography blocking
6 experiments including correlation studies with immunohistochemistry staining. **However**, such
7 techniques do not investigate tracer enrichment on the cellular level. Nevertheless, this is of
8 particular interest, when the specificity of a novel tracer has to be explored or when the
9 radioactivity distribution is to be assigned to specific cell types. **In neuroinflammatory tissue,**
10 **the discrimination of tracer accumulation in different microglia phenotypes could be of eminent**
11 **importance. Such approaches could support the development of specific ligands for**
12 **homeostatic and disease-associated microglia which would facilitate monitoring of therapeutic**
13 **agents that modulate distinct microglia phenotypes.** In principle, scRadiotracing could be
14 applied to any radiotracer binding to an intracellular target. However, it is questionable if
15 ligands of membrane bound targets on the surface of cells also qualify for scRadiotracing
16 analysis. Upstream cell processing promises a gentle mechanical and enzymatic dissociation
17 preserving cell integrity and surface epitopes, but it has to be proven if high affinity binders
18 withstand hydrolytic treatment. This also applies to subsequent downstream applications
19 beyond quantification in a gamma counter. In this respect, ligands showing a high
20 internalization rate, may be most likely applicable to scRadiotracing analysis.

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22 **Methodological limitations and considerations**

23 First, we note the difficulty to quantify the uptake of a whole cell population via
24 scRadiotracing. The procedure of cell dissection and harvesting may over- or underestimate
25 the proportion of viable cells of the brain or in specific regions (22), which hampers
26 extrapolation to absolute cell numbers. Cell proportions can also be influenced by proliferation
27 and cell loss which lead to subsequent alterations in cell density. Thus, scRadiotracing

1 facilitates robust calculation of radiotracer uptake per cell, but extrapolation to the whole
2 fraction is erroneous. One possibility to establish a full allocation model of radiotracer uptake
3 per cell type and fraction could be established by simultaneous light sheet microscopy (23).
4 Light sheet microscopy offers the possibility to quantify the absolute amount of cells per cell
5 type in a 3-dimensional volume, i.e. by analysis of a subsample of the target.

6 Unlike well-established nearly irreversibly bound 18F-FDG, all non-18F-FDG
7 radioligands may suffer from higher instability during the scRadiotracing procedure. For
8 instance, the binding stability of a TSPO ligand to the TSPO complex at the mitochondrial
9 membrane could decrease during the scRadiotracing procedure. This also accounts for current
10 tau-ligands like 18F-PI-2620 which is characterized by a decrease of target-bound radiotracer
11 over time in 4-repeat tauopathies (24).

12 Loss of processes and synapses potentially impact quantitative results of
13 scRadiotracing. 18F-FDG in neuronal synapses comprises one important example of missed
14 radiotracer in the scRadiotracing workflow (7,9). Optimization of the dissociation procedure
15 has the potential to further enhance the accuracy of scRadiotracing. In similar regard,
16 consideration of live and dead cells may stabilize scRadiotracing results since cells with leaky
17 membranes can be excluded.

18 Cell separation after TSPO tracer injection was also proposed by a recent study using
19 a similar technique of fluorescence activated cell sorting (FACS) to determine the cellular
20 source of a 125I labelled single photon emission computed tomography (SPECT) TSPO ligand
21 (125I-CLINDE) (25). Here, the long half-life of 125I offered the opportunity to conduct the
22 experiments with less time constraints. When comparing both approaches, MACS systems
23 can be installed relatively simple within a radiation protection controlled area and the higher
24 cell yield is another advantage of MACS over FACS, which even allows to perform proteomic
25 analyses (26). On the other hand, FACS offers the advantage of direct separation of genetically
26 determined fluorescent cells (i.e. GFP) which cannot be achieved via MACS. Furthermore,
27 specific cell populations, such as homeostatic or disease associated microglia, can be selected

1 via FACS gating, when discriminative antibodies are used. Considering the stability of
2 radiotracer binding once more, there is a need to investigate the impact of emitted energy
3 during cell sorting via FACS, which could be of high relevance for tracers bound at voltage
4 channels. Head-to-head comparisons of both approaches will be required to allow
5 recommendations on a preferential use of MACS or FACS systems for scRadiotracing.

6 scRadiotracing in human tissue after *in vivo* or *in vitro* tracer application comprises
7 another promising methodological variant (25). *In vitro* application of radiotracer to tissue
8 allows to investigate small amounts of tissue which do not yield a sufficient signal-to-noise ratio
9 when the tracer is applied *in vivo* (i.e. prior to surgery of tumors). However, scRadiotracing
10 after tracer application *in vivo* could be used to validate *in vitro* scRadiotracing in the same
11 tissue when amounts are large enough. Furthermore, blocking with cold ligands could be
12 performed to test for the specificity of cellular radiotracer binding using *in vitro* scRadiotracing.
13 **As a limitation, we note that the extensive work flow (see Fig.1) likely restricts scRadiotracing**
14 **to an experimental setting but prevents it from use in clinical routine at the current stage.**

15 In summary, we highlighted some of the broad range of highly demanded applications
16 for the novel scRadiotracing workflow to elucidate tracer uptake mechanisms and their
17 underlying cell biology.

18

19 **Noteworthy**

- 20 • Cellular sources of ¹⁸F-FDG and other PET imaging radiotracers are poorly
21 understood (page 2, line 11-17)
- 22 • Immunomagnetic cell sorting after radiotracer injection (scRadiotracing) facilitates
23 determination of *in vivo* radiotracer uptake per specific single cell (page 2, line 18-22)
- 24 • scRadiotracing is of high interest when radiotracer targets are expressed and
25 pathologically altered on different cell types, such as applicable for 18kDa
26 translocator protein (TSPO) (page 4, line 8-12)

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Figure Caption

Figure 1 - Workflow of single cell radiotracer allocation via immunomagnetic sorting (scRadiotracing) to determine microglial 18F-FDG uptake in brain at cellular resolution:

After tracer injection into the tail vein, the brain is removed upon a tracer specific uptake period. Following the generation of a single cell suspension, immunomagnetic cell separation is used to separate fractions of enriched cells and their depleted counterparts, which contain bound radioactivity. Fluorescent labeling, gamma counting and flow cytometry are used to calculate radioactivity per cell as the primary read-out. Time necessary to complete each experimental step is indicated together with the summed timed during the workflow. p.i. = post injectionem. CD11b is used to detect microglia. Copyright © 2022 Miltenyi Biotec B.V. & Co. KG. All rights reserved.

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Disclosure

The authors do not indicate a conflict of interest